Vulnerable Atherosclerotic Plaque: From the Basic Research Laboratory to the Clinic

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Key Words
Vulnerable plaque · Thin-cap fibroatheroma · Intravascular imaging · Intravascular ultrasound · Optical coherence tomography · Intravascular thermography

Abstract
Coronary heart disease is the commonest cause of death in Western countries, and atherosclerotic plaques that are prone to rupture have been implicated in the pathogenesis of acute coronary syndromes (ACS). Intensive research has been directed at plaque detection, and various invasive methods have been developed thus far that fulfill this purpose and a lot of them are being applied in the clinical setting. Since invasive methods cannot be used for primary prevention, non-invasive imaging modalities are being studied to enhance the diagnostic armory of clinicians in their difficult task of detecting and preventing ACS.

Introduction
Coronary heart disease remains the single most common cause of death in the European Union and the USA, even though there has been a reduction in the crude number of coronary heart disease deaths when compared with the previous decade [1, 2]. Atherosclerosis is usually complicated by acute thrombosis, which is triggered by the rupture or erosion of an atherosclerotic plaque, which in turn leads to acute ischemic events. The Framingham risk equation [3] and the Systematic Coronary Risk Evaluation system [4] are currently being used to identify high-risk patients and predict the risk of a future acute coronary syndrome (ACS). However, these scores accurately estimate the cardiovascular risk of middle-aged men but tend to significantly underestimate that of younger patients [5, 6]. The rupture of an unstable coronary atherosclerotic plaque usually precedes a majority of acute cardiovascular events [7]. Since most acute events are caused by the rupture or erosion of nonhemodynamically significant plaques rather than the progression of flow-limiting lesions [8], indicating that the predictive value of noninvasive stress testing for predicting acute vascular events is particularly poor, the need to develop new diagnostic tools that focus on de-
tecting rupture-prone plaques is emerging. The purpose of this review is to focus mainly on the intravascular modalities that are being used and to briefly assess the existing noninvasive imaging modalities used for coronary plaque detection.

**Vulnerable Plaque Concept**

During the past decade, identification of plaques likely to cause an acute event in the future has been a topic of intensive research. The term vulnerable plaque denotes a plaque that is more prone to lead to ACS. Although such events could be triggered by plaque rupture, plaque erosion or plaque disruption due to calcified nodules, the pathophysiology of the latter mechanisms is currently poorly understood [9, 10]. Thus, most attempts to identify vulnerable plaques have focused on the identification of rupture-prone plaques. Histological characteristics of such plaques include the presence of a thin fibrous cap (≤65 μm), large necrotic core, expansive remodeling, increased neovascularization and infiltration of the fibrous cap by activated macrophages [11]. The type of plaque that is associated with these features is called a thin-cap fibroatheroma and is considered the precursor of a ruptured plaque.

**Invasive Imaging Modalities**

There are various intravascular imaging modalities that have been used in an attempt to identify vulnerable atheromatic plaques, in animal and human studies, each of them having its own advantages and drawbacks.

**Intravascular Ultrasound**

Grayscale intravascular ultrasound (IVUS), being the first invasive method used for imaging of the vascular wall, has been applied for vulnerable plaque characterization. It can assess plaque burden and the presence of expansive remodeling, which constitute two important features of plaque vulnerability, and it can classify atheromatic plaques as soft, fibrous, calcified or mixed, without, however, being able to assess the actual histologic composition [12]. However, the limited resolution does not allow for accurate tissue characterization or for identification of the most crucial components of vulnerable plaque, i.e. necrotic core content and fibrous cap thickness. These limitations have led to the development of signal processing methods such as virtual histology IVUS (VH-IVUS) and integrated backscatter IVUS (IB-IVUS) that use signal processing methodologies in order to assess the tissue composition of the plaque.

**Virtual Histology IVUS**

VH-IVUS uses a mathematical autoregression model, and the results of this analysis are displayed as a color-coded map. Plaque components are usually categorized into 4 tissue types: fibrous, fibro-fatty, calcified and calcified necrotic [13, 14]. The diagnostic accuracy of VH has been validated against histology, thus enabling the differentiation of the various components of the plaque under study.

The Providing Regional Observations to Study Predictors of Events in the Coronary Tree (PROSPECT) trial was a natural-history study using multimodality imaging of the entire coronary tree that showed that approximately 20% of patients with ACS treated with stents and optimal medical therapy developed major adverse cardiac events within 3 years, and 12% of these patients developed events from nonculprit lesions [15], the same rate as in culprit lesions.

**Integrated Backscatter IVUS**

IB-IVUS was developed in order to overcome the limitations of grayscale IVUS. The IB values of the different tissue components can be used to generate a color-coded IB-IVUS image. Both ex vivo [16, 17] and in vivo [18] studies have validated the accuracy of this approach. An autopsy-based study of 42 coronary specimens showed the sensitivity of IB-IVUS for calcification, fibrous and lipid-rich plaque to be 100, 94 and 84%, respectively, which compares favorably with optical coherence tomography (OCT; 100, 98 and 95%, respectively) and conventional IVUS (100, 93 and 67%, respectively) [19]. When compared with VH-IVUS, IB-IVUS provided higher diagnostic agreement with histological assessment [20].

**Elastography and Palpography**

Elastography and palpography are methods utilizing IVUS-derived data that assess the local strain of the vessel wall and plaque. A color-coded map is obtained that shows areas with high mechanical strain. High-strain regions denoting vulnerable plaques detected by these two methods have been identified in experimental models and in humans [21]. The recent publication of the palpography arm of the PROSPECT trial has shown that the predictive value of palpography for detection of future events is fairly limited [22].
Coronary Angioscopy

Coronary angioscopy allows the visualization of the inner surface of the vessel and concomitantly the atherosclerotic plaque. The intensity of the yellow color detected (slight yellow, yellow, intensive yellow) is used for plaque characterization [23], and intense yellow color of the plaque has been linked with ACS. However, coronary angiography is unable to provide details regarding the interior of the plaque, rendering its use futile.

Optical Coherence Tomography

OCT is a light-based imaging modality able to visualize the majority of the morphological characteristics of the vulnerable plaque, including the type of plaque, the lipid core size, the exact thickness of the fibrous plaque [24, 25], neovascularization and plaque infiltration by macrophages [26], and can also provide precise morphological assessment of the ruptured plaque and not only detect the presence and extent of thrombosis but characterize the type of thrombus as well [27–29]. The combined use of OCT and VH-IVUS has shown encouraging results [30], and further studies with the combined usage of these modalities are warranted.

Furthermore, OCT has provided useful insights into the localization of high-risk plaques. An in vivo OCT study has shown that 76% of thin-cap fibroatheromas were found on the first 30 mm from the left anterior descending artery orifice [31]. These results have been confirmed by other studies, where culprit lesions of ACS patients located in the proximal segments of the left anterior descending artery have a thin fibrous cap and increased incidence of plaque rupture compared to distal culprit lesions [32].

Limitations of OCT include limited penetration that allows for imaging of the superficial 1.5–2 cm of the plaque surface but does not allow the precise assessment of plaque burden and the remodeling index. Nevertheless, the majority of the 'vulnerable' morphological characteristics are located near the surface of the plaque, while the introduction of second-generation OCT systems with high-speed image acquisition in clinical practice helps overcome limitations of first-generation systems that required prolonged displacement of the blood from the studied artery.

Near-Infrared Spectroscopy

Near-infrared spectroscopy (NIRS) evaluates the spectrum of absorption of near-infrared light with different wavelengths by different tissue components in order to identify the chemical composition of the substance. A color-coded map is formed where yellow corresponds to high probability and red corresponds to low probability of lipid-core plaque. Recently, in an autopsy study, NIRS was used successfully to identify lipid-core plaques and correlated well with histology [33]. A combined NIRS-IVUS catheter has also been used that enables both plaque architecture and composition identification, thus enabling culprit and nonculprit lesion identification and stent length selection [34]. Nonetheless, this combined catheter has yet to be tested in a larger cohort, and further results are awaited.

Intravascular Thermography

Ex vivo specimens of atherosclerotic plaques have been shown to be associated with thermal heterogeneity, as a result of heat production by macrophages, and thus thermal heterogeneity can be used as a surrogate marker for detection of heavily inflamed plaques. In the first-in-man study of an intravascular catheter for the assessment of thermal heterogeneity in atherosclerotic plaques, culprit plaques of patients with ACS were found to have higher temperature differences compared to those in patients with stable angina [35]. Furthermore, a prospective study in 86 patients undergoing a percutaneous coronary intervention showed that increased local temperature in atherosclerotic plaques is a strong predictor of unfavorable adverse events [36]. Another study using thermography and IVUS has shown that the site with the highest temperature is distal to the angiographically most stenotic site [37], accurately localizing the culprit lesion. Furthermore, combined plaque assessment by IVUS and thermography has shown that plaques with expansive remodeling and ruptured plaques are associated with increased local inflammatory activation, as demonstrated by an increased temperature difference [38]. The use of thermography for vulnerable plaque detection is limited due to the cooling effect of blood flow that causes underestimation of temperature differences and due to the need for the tip of the catheter to be in contact with the vessel wall being studied [39], which could lead to vessel damage.

Noninvasive Imaging

The development of noninvasive modalities for the detection of the vulnerable plaque has been the subject of intensive research interest. However, despite technological advancements, noninvasive imaging modalities still have poor sensitivity, specificity and resolution and so they cannot detect the features of the vulnerable plaque.
**Multidetector Computed Tomography**

The accuracy of multidetector computed tomography has increased, as has the ability to imagine the vessel wall [40]. The multidetector computed tomography criteria for plaque vulnerability have been validated against VH and OCT in ACS patients [41–43], as well as in plaques which were not heavily calcified [42].

**Magnetic Resonance Imaging**

MRI is usually applied for large and static arteries, since the continuous motion of the coronary arteries remains an obstacle for imaging them. Furthermore, the poor reproducibility of MRI is the main restriction for vulnerable plaque detection [44], whereas newer studies have showed that high-intensity plaques lead to ischemic events [45].

**Nuclear Imaging**

Nuclear imaging modalities, such as single-photon emission computed tomography and positron emission tomography, have also been extensively studied. Positron emission tomography has a better resolution and less diagnostic uncertainty, so it has been used in most of the studies on nuclear imaging of atherosclerosis [46]. $^{18}$F-labeled fluorodeoxyglucose is a tracer currently being used for detecting metabolically active cells. In humans with carotid atherosclerosis [47], areas of high $^{18}$F-labeled fluorodeoxyglucose uptake have been shown to colocalize with areas of macrophage accumulation, irrespective of plaque size or luminal narrowing.

**Contrast-Enhanced Ultrasonography**

Contrast-enhanced ultrasonography has been used for imaging the inflammatory response by detecting vascular cell adhesion molecule-1 in the aorta [48], which allows for the monitoring of the various atherosclerosis stages.

**Microwave Radiometry**

Microwave radiometry (MR) is a novel method that measures natural electromagnetic radiation from a patient’s internal tissues at microwave frequencies. MR has been used previously to detect temperature changes in breast cancer patients. Recently, MR was applied to an experimental hypercholesterolemic model, and thermal heterogeneity was measured with both MR and intravascular thermography. The results showed good correlation between the two methods, as well as with the histological findings [49].

After experimental demonstration, MR was tested in vivo in patients with carotid artery disease who were scheduled for endarterectomy. Besides MR measurement, these patients also underwent carotid echocardiography and histological and immunohistochemical studies following endarterectomy. The results were encouraging, as they revealed a positive correlation of the MR temperature measurements with the echocardiographic characteristics of the vulnerable plaques [50].

**Future Perspectives**

Currently, there is no imaging method that can properly assess all the aspects of plaque vulnerability. Moreover, each modality has its own advantages and disadvantages. An imaging modality that can be used for vulnerable plaque detection needs to be safe, efficient and ideally cost-effective. Due to their invasiveness and high cost, intravascular methods cannot be used as a screening tool for the general population. Moreover, their use in high-risk individuals cannot be justified because (1) besides the PROSPECT trial there are currently no other large-scale natural-history studies providing proof of a potential improvement in patient-related outcomes by using intravascular imaging for the detection of high-risk plaque, (2) the high-risk morphological characteristics that are more crucial for the determination of plaque vulnerability and consequently the ideal modality for vulnerable plaque detection have not been identified and (3) the dynamic changes in plaque morphology, principally affected by local rheological conditions, make morphological assessment alone insufficient for the determination of vulnerable plaque.

Consequently, the development of a modality able to detect vulnerable plaques will have to focus not only on the assessment of morphology but also on the functional assessment of the plaque. A combination of morphological assessment by OCT with shear stress assessment could perhaps be applied for vulnerable plaque characterization in very high-risk individuals already treated with intensive medical therapy. The development of new therapeutic tools dedicated to the passivation of vulnerable plaques could potentially fulfill the expectation of local treatment of these plaques and allow prevention of future events.

Furthermore, the development of noninvasive methods that will be able to provide imaging biomarkers of plaque vulnerability could improve risk stratification on a population-level basis and identify individuals in need of intensive treatment.
Invasive imaging is still the cornerstone for imaging and detecting the vulnerable plaque, while noninvasive imaging modalities have an increasingly important role in detecting the vulnerable plaque or conditions associated with coronary heart disease and can be of great value and assistance in addition to invasive modalities.

References


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Cardiology 2012;123:248–253


