Effect of Percutaneous Ventricular Assist Devices on Renal Function

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Introduction

Cardiovascular diseases (CVD) are the major cause of death worldwide [1]. In the USA, the 2007 overall death rate from CVD was 251.12 per 100,000 individuals [2]. Various therapeutic strategies for CVD are available, from lifestyle changes and medication to mechanical circulatory support. A ventricular assist device (VAD) can be used to improve the systemic circulation and to decrease the load on the myocardium prone to heart failure refractory to pharmacologic therapy. Depending on the method of VAD placement, a VAD can be categorized as a percutaneous device or as an implantable device. During an acute critical event, percutaneous devices are preferred due their rapid deployment since implantable devices require more extensive procedures. Implantable devices, however, are used for end-stage heart failure patients as a bridge to heart transplantation, recovery or destination therapy [3, 4].

Placement of a VAD has the potential to improve internal organ function by preventing or reversing organ hypoperfusion and allowing organ recovery [5]. Potentially, the use of a VAD could be associated with acute
organ failure [6]. Interaction mechanisms between VAD and internal organs have been hypothesized [7–10]. Renal function prior to VAD placement is a predictor of clinical outcome. Optimal benefit from a VAD depends on balancing the interaction mechanisms between the VAD and the kidney during the pre-, intra- and postoperative periods. In their review of renal failure in patients treated with a left VAD (LVAD), Patel et al. [11] noted that significant number of patients with end-stage heart failure refractory to conventional medical therapy had renal dysfunction prior to LVAD implantation. The risk of acute kidney injury after LVAD implantation is reported to be 7–56%. On the other hand, renal function may be improved after LVAD implantation, as measured by serum creatinine, creatinine clearance and estimated glomerular filtration rate (GFR). To assist in clinical decision-making, we reviewed mechanical principles and clinical studies of percutaneous heart-assist devices (intra-aortic balloon pump (IABP) Impella, TandemHeart and Cardiobridge) to address the potential renal effects of these devices. Because the focus of this study is set on the renal effects of devices dedicated to cardiac support only, extracorporeal membrane oxygenation systems are not included.

**Clinical Indications**

Although cardiac transplantation offers the best possible solution for patients with severe heart failure, many patients succumb to their disease while waiting for a transplant due to the high number of patients on the waiting list and the low number of transplants available. Therefore, the use of VADs, especially percutaneous VADs, has increased, since they have the advantages of rapid deployment and widespread availability.

In the following, the major indications for VADs are listed.

**Cardiogenic Shock.** Mortality from cardiogenic shock (CS) complicating acute myocardial infarction (AMI) is as high as 60–70% [12]. VAD use can result in significantly increased cardiac output (CO) and consequently end-organ perfusion. In turn, this diminishes the systemic inflammatory response syndrome that can add to the cardiac dysfunction. Delayed treatment of CS can lead to multiorgan failure. Some studies have reported that percutaneous VAD (pVAD) treatment improved CO by 37–43% [13, 14]. Differences in survival are key determinants in the design and analysis of VAD studies. **Bridging.** Patients who are placed on a waiting list for a donor heart may require either temporary [15] or long-term VAD placement as a bridge to transplantation or to recovery per se. In the meantime, complications related to coronary artery disease, such as the postcardiotomy syndrome and myocarditis, can be addressed.

**High-Risk Percutaneous Coronary and Valvular Interventions.** Patients with severe left main coronary stenosis, either due to hemodynamic instability or comorbidities, have been shown to be at increased risk during percutaneous coronary interventions (PCI). The benefits of percutaneous ventricular support have been documented in a retrospective study of 144 patients by the Europella Registry [16] and in PROTECT II, a randomized controlled study including 305 patients [17].

**Ventricular Tachycardia Ablation.** The major advantage of a pVAD in this setting is the maintenance of hemodynamic stability during and early after the procedure. Without such a device, hemodynamic instability may preclude performance of an ablation procedure [18].

There is limited experience with regard to the use of pVADs in patients with right ventricular failure. However, successful treatment with a percutaneous right VAD (TandemHeart) has been described [19, 20]. Overall, the major indications for pVADs are the need to treat CS when medical treatment combined with IABP is not sufficient, and the need to create stability during high-risk procedures. pVADs have the potential to provide stability while the patient is awaiting surgical long-term support or transplantation, especially in patients with profound hypotension and a high risk of mortality.

**Percutaneous Devices and Renal Function**

Several pVADs are available for mechanical circulatory support in the catheterization laboratory. The most widely used devices are the IABP, the TandemHeart system and the Impella 2.5. A number of novel pVADs have recently been developed, such as the Cardiobridge (Reitan catheter pump (RCP)). A comparison of the pVADs available is listed in table 1.

**Intra-Aortic Balloon Pump**

The IABP has been the most widely used pVAD since its introduction in 1968 [21] and is frequently the first assist device used in CS treatment. In the community setting, an IABP is generally inserted percutaneously via the femoral artery. The balloon is then positioned in the descending aorta, just distal to the left subclavian.
artery and well proximal to the renal arteries (fig. 1a). When balloon inflation occurs at the start of diastole and deflation before systole, the IABP can augment CO by 0.3–0.5 ml/min [22] depending on a stable native cardiac rhythm, the balloon volume, the aortic compliance and systemic vascular resistance. Studies have demonstrated its effect on CO and significant improvement in systemic perfusion due to increased diastolic pressure, decreased left ventricle (LV) end-diastolic pressure and decreased oxygen demand induced by the decrease in afterload and ventricular wall tension [23]. However, an IABP may not provide adequate circulatory support for patients with severe CS or hemodynamic instability due to severe cardiac arrhythmias. Thiele et al. [24] have addressed IABP use in patients with myocardial infarction with CS. The use of an IABP for CS after ST-segment elevation myocardial infarction has a class I guideline recommendation [25]. The reported morbidity rate related to IABP insertion is 8.7–29% [26, 27], but there is no significant association between IABP-related complications and short- or long-term mortality [28, 29].

Renal dysfunction associated with cardiac surgery influences short- and long-term mortality [30, 31]. Factors such as perioperative hypotension, use of potential nephrotoxic therapeutic agents, radiopaque contrast media, cardiopulmonary bypass and IABP have been identified as factors contributing to renal dysfunction associated with cardiac surgery [32]. In a multivariate model, the preoperative patient characteristic most strongly associated with postoperative severe renal insufficiency (estimated GFR <30 ml/min/1.73 m$^2$) was preoperative IABP use [30, 33]. Interpretation is difficult, as use of an IABP usually indicates a severe clinical state. Clinicians

**Table 1. Comparison of PVADs currently available**

<table>
<thead>
<tr>
<th></th>
<th>IABP</th>
<th>Impella 2.5</th>
<th>TandemHeart</th>
<th>Cardiobridge</th>
</tr>
</thead>
<tbody>
<tr>
<td><strong>Mechanism</strong></td>
<td>pneumatic</td>
<td>axial flow</td>
<td>centrifugal</td>
<td>centrifugal</td>
</tr>
<tr>
<td><strong>Position</strong></td>
<td>balloon catheter in the descending aorta via the femoral artery</td>
<td>catheter across the aortic valve into LV via the femoral artery</td>
<td>inflow cannula into the left atrium via the femoral vein and transseptal puncture and outflow via cannula in the femoral artery</td>
<td>pump head deployed in the descending aorta via the femoral artery</td>
</tr>
<tr>
<td><strong>Insertion time</strong></td>
<td>+</td>
<td>+++</td>
<td>++++</td>
<td>++</td>
</tr>
<tr>
<td><strong>Increase CO, l/min</strong></td>
<td>0.5</td>
<td>2.5</td>
<td>3.5-4.5</td>
<td>5</td>
</tr>
<tr>
<td><strong>Anticoagulation</strong></td>
<td>+</td>
<td>+</td>
<td>+</td>
<td>+</td>
</tr>
<tr>
<td><strong>Need heart synchronization</strong></td>
<td>yes</td>
<td>no</td>
<td>no</td>
<td>no</td>
</tr>
<tr>
<td><strong>Limb ischemia</strong></td>
<td>+</td>
<td>++</td>
<td>+++</td>
<td>++</td>
</tr>
<tr>
<td><strong>Hemolysis</strong></td>
<td>0</td>
<td>++++</td>
<td>++</td>
<td>+</td>
</tr>
<tr>
<td><strong>Bleeding</strong></td>
<td>+</td>
<td>++</td>
<td>+++</td>
<td>+</td>
</tr>
<tr>
<td><strong>Cardiac outcome</strong></td>
<td>decreased afterload, LVED pressure, ventricular wall tension; increased CO and coronary and peripheral perfusion</td>
<td>decreased PCWP; increased CO and MAP</td>
<td>decreased PCWP, MPAP, CVP; increased CO, MAP and Mvo2</td>
<td>increased femoral pressure, decreased radial pressure</td>
</tr>
<tr>
<td><strong>Renal outcome</strong></td>
<td>increased renal blood flow, decreased VEGF, MCP-1 and cytokines</td>
<td>decreased lactic acid</td>
<td>increased urine output, decreased sCr and BUN</td>
<td>increased urine output, decreased sCr and BUN</td>
</tr>
</tbody>
</table>

BUN = Blood urea nitrogen; CVP = central venous pressure; LVED = LV end-diastolic pressure; MAP = mean arterial pressure; MCP-1 = monocyte chemotactic protein-1; MPAP = mean pulmonary arterial pressure; Mvo2 = mixed venous oxygen saturation; PCWP = pulmonary capillary wedge pressure; sCr = serum creatinine; VEGF = vascular endothelial growth factor.
are faced with the question whether the use of an IABP is safe for patients with renal failure.

The effect of the IABP on renal blood flow in high-risk patients was studied by Sloth et al. [1]. They found that renal artery diameters were unchanged, and that there was no decrease in renal resistance and/or compliance. Interlobar renal blood flow was higher during IABP treatment measured by Doppler ultrasound, without a simultaneous change in creatinine clearance. In a study of the use of an IABP during cardioplegic arrest, Onorati et al. [34] found that IABP use induced hemodynamic improvement which resulted in lower serum IL-2 and IL-6 and higher IL-10 levels, lower endothelial markers (vascular endothelial growth factor and monocyte chemotactic protein-1) [35] together with improved estimated GFR, lower creatinine from admission to the intensive care unit to 48 h in patients with preoperative kidney disease of stages 1–2 and 3. The incidence of renal insufficiency and the need for renal replacement therapy were also lower in stage 3 IABP. IABP-induced pulsatile flow was also found to improve whole body perfusion including renal function in the elderly undergoing cardiopulmonary bypass surgery [36].

Muniraju et al. [37] reported a prospective observational study of the use of a preoperative IABP in patients undergoing elective off-pump coronary artery bypass surgery. They found no change in serum creatinine from the baseline value of 1.10 ± 0.23 to 0.98 ± 0.363 mg/dl (p < 0.05). Cystatin C levels were significantly decreased from the baseline level of 0.98 ± 0.29 to 0.89 ± 0.23 (p < 0.05). Lack of an elevation in cystatin C levels also suggested absence of potentially IABP-induced renal dysfunction in patients on elective IABP therapy preoperatively. Recently, in a randomized, prospective, open-label, multicenter trial including 600 patients, IABP use did not significantly reduce 30-day mortality and resulted in no difference in renal function in patients with CS complicating AMI for whom an early revascularization strategy was planned [24].

Impella

The Impella® Recover®LP Support System (AbioMed) is a continuous-flow, microaxial blood pump designed for rapid institution of temporary circulatory support. Two models are available, Impella 2.5 and Impella 5.0. The former can provide up to 2.5 l/min and can be percutaneously inserted, whereas the latter can deliver up to 5.0 l/min, but requires a surgical incision for insertion into a peripheral artery or directly into the ascending aorta. The Impella is positioned across the aortic valve in the LV. The Impella pump aspirates blood from the LV and pumps it into the ascending aorta (fig. 1b). The amount of flow depends on the rotation speed (max. 32,000 rpm) and on the pressure gradient between the aorta and the LV. The Impella 2.5 is FDA approved for up to 6 h of partial circulatory support. The Impella directly unloads the LV which results in increased CO and mean arterial pressure and decreased pulmonary capillary wedge pressure and lactic acid levels [14, 38]. Several studies have shown that Impella is effective and safe in ST-segment elevation myocardial infarction and high-risk PCI patients [39, 40]; however, experience in CS patients

Fig. 1. a IABP: it is inserted in the femoral artery and the balloon is positioned in the descending aorta distal to the left subclavian artery and proximal to the renal artery branches. b Impella 2.5: it is positioned across the aortic valve in the LV, aspirates blood from the LV and pumps it into the ascending aorta. c TandemHeart: it aspirates oxygenated blood from the left atrium via a transeptal cannula placed in the femoral vein and returns blood via the femoral artery to the lower abdominal aorta. d Cardiobridge: it is positioned in the descending aorta and creates a pressure gradient.
is limited [14], and there are no data that demonstrate a reduction in mortality rates [41].

From a physiologic point of view, kidney function should improve after pVAD implantation if the baseline renal dysfunction is secondary to low CO, poor renal perfusion or renal venous congestion. However, there is no study investigating renal function changes after Impella implantation in a large patient cohort. In a case report which included 3 patients who underwent high-risk coronary angioplasty, use of the Impella 2.5 system resulted in an increase in serum creatinine of 1 mg/dl (from 1.8 to 2.8 mg/dl). The author analyzed the renal dysfunction due to contrast medium (mean amount of 323 ml) [42]. In another study, the Impella 2.5 was implanted in patients with CS (n = 6) or in patients undergoing high-risk PCI (n = 5). Renal failure was observed in 4 patients, all of whom had CS [43]. Considering the complicated clinical condition and limited sample size, it could not be concluded that the use of the Impella 2.5 has a potential adverse effect on renal function. In another study, use of the Impella 5.0 in 5 patients with CS and severe renal failure with oliguria or anuria was associated with hemodynamic improvement, and a decrease in mean serum creatinine level from 176.8 to 79.6 µmol/l 15 days after implantation (p = 0.02) [44].

Use of the Impella has been associated with increased levels of hemolysis and its secondary effects. A higher incidence of hemolysis has been reported in patients treated with an Impella versus an IABP [41]. Acute kidney injury secondary to severe hemolysis after Impella 2.5 placement has been reported [45]. In patients who develop hemolytic anemia after Impella insertion, urinary output and renal function should be closely monitored. Cannula position should be evaluated, and the flow reduced as tolerated. The device should be removed as early as possible to reduce the extent of hemolysis and preserve renal function.

**TandemHeart**

The TandemHeart is a continuous-flow, extracorporeal pump that can provide temporary support from a few hours up to 14 days, to facilitate cardiac recovery. The TandemHeart aspirates oxygenated blood from the left atrium via a transseptal cannula that has been placed in the femoral vein. The pump returns blood to the femoral artery or lower abdominal aorta establishing a left-atrial-to-femoral arterial bypass (fig. 1c). The pump has an internal system of continuous heparin administration via the device lubrication system to reduce the need for systemic anticoagulation. At the maximum rotational speed of 7,500 rpm, the TandemHeart can deliver blood flow up 4–5 l/min. The system is used in CS complicated by AMI and in high-risk PCI. Studies have demonstrated that the TandemHeart can increase the cardiac index, blood pressure, mixed venous oxygen saturation, urine output and reverse hemodynamic instability with subsequent decreases in pulmonary capillary wedge pressure, mean pulmonary arterial pressure and central venous pressure [13, 46]. The major risks of the TandemHeart are bleeding and limb ischemia.

There are few studies investigating changes in renal function after TandemHeart support. The TandemHeart has been compared with IABP support in 41 patients with revascularized AMI complicated by CS [13]. The cardiac power index was more effectively improved by the TandemHeart and was accompanied by a more rapid decrease in serum lactate and improved renal function. However, there were no significant differences with respect to 30-day mortality, and complications, including limb ischemia and severe bleeding, were more frequent with the TandemHeart than with IABP support.

With regard to renal function, in a study of TandemHeart implantation during high-risk PCI, Aragon et al. [47] reported that 1 of 8 patients developed acute renal failure after the procedure and required hemodialysis. Gregoric et al. [48] studied 8 patients with cardiac arrest or severe refractory CS receiving TandemHeart support for 6.4 ± 3.8 days before aortic valve replacement for critical aortic valve stenosis in the catheterization laboratory and noted significant improvement in renal function with decreases in serum creatinine (2.0 ± 0.9 to 1.1 ± 0.3 mg/dl; p = 0.002) and blood urea nitrogen (46.5 ± 26.5 to 28.9 ± 13.3 mg/dl; p = 0.023). Before pVAD placement, 6 of the 8 patients were anuric, whereas during TandemHeart support, urine output improved and reached 155 ± 78 ml/h. While improvement in hemodynamic parameters by the TandemHeart appears promising, it remains to be determined whether this benefit translates into reversed organ dysfunction and improved clinical outcomes.

**Cardiobridge (RCP)**

The Cardiobridge support device (RCP) is a continuous nonphasic pump that consists of a catheter-mounted pump head with a foldable propeller and surrounding cage (fig. 1d). Its unique foldable propeller mechanism allows for percutaneous insertion. Positioned in the descending aorta, the pump creates a pressure gradient, reduces afterload and enhances organ perfusion. The pump functions without the need for heart synchronization and is not limited by the state of the aortic valve (native or prosthetic). The RCP is not positioned within the LV cavity and therefore is not contraindicated in the presence of LV thrombus.
Smith et al. [49] reported a first-in-man study of the RCP implanted in 10 consecutive patients requiring circulatory support who underwent PCI. RCP was inserted via the femoral artery before PCI and was removed 1–6 h after the procedure. The pump operated successfully in 9 of 10 cases (median 79 min). There was no significant hemolysis, and platelet counts were unchanged. Baseline serum creatinine (before RCP) fell during a mean of 11 ± 8 μmol/l (p = 0.004) and a corresponding increase in GFR from 66.7 ± 18.1 to 74.9 ± 23.6 ml/min.

In an unpublished study (author communication) of the hemodynamic efficacy of RCP in patients with acute decompensated chronic heart failure, the RCP brought about a rapid and marked diuresis. Urine output increased from a baseline of 54 ml/min to 213 ml/h after 12 h (p = 0.029). Serum creatinine fell from 193 to 151 μmol/l at 12 h (p = 0.003, 22% reduction). Further study of this device which has promising early results is needed.

Chronic Renal Disease

In the acute-care setting, for example CS treatment, it is not possible to distinguish renal dysfunction that occurs as a result of acute hypoperfusion from renal dysfunction related to preexisting chronic kidney disease. Consequently, delay in restoring organ perfusion or addressing a nephrotoxic event, such as contrast medium exposure or hemolysis, can slow recovery of renal function or lead to irreversible damage and the associated worse outcomes. It is of note that nearly two thirds of hospitalized patients with heart failure also have chronic kidney disease and are less likely to receive important guideline-recommended therapies [50].

Conclusion

The major indications for pVADs are hemodynamic instability due to acute heart disease, the threat of hemodynamic instability during high-risk PCI and valvular interventions, and the need for a temporary bridge to heart transplantation or an implantable VAD. An important consequence of hemodynamic instability and CS is end-organ hypofusion with resulting injury. Low urine output, a marker of kidney hypoperfusion, is one of the criteria used to define CS and is well known to be associated with worse outcomes. pVAD insertion with hemodynamic improvement should improve kidney function as a result of the restoration of perfusion. However, there are only a few studies reporting the effect of pVADs on kidney function, and the patient numbers studied are small. Nevertheless, the available clinical data support pVAD as a means to reverse and prevent renal failure in patients with marked hemodynamic compromise. In that kidney function is one of the most reliable predictors of outcome in the setting of acute heart disease, the pVAD should be chosen depending on its expected renal effects.

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Disclosure Statement

All of the authors declare no competing interests.

References

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