Blood Bag Plasticizers Influence Red Blood Cell Vesiculation Rate without Altering the Lipid Composition of the Vesicles

Beatriz Bicalho a, Katherine Serrano b, c, Alberto dos Santos Pereira d, Dana V. Devine b, c, Jason P. Acker a, d

a Canadian Blood Services, Center for Innovation, Edmonton, AB, Canada; 
b Canadian Blood Services, Center for Innovation, Vancouver, BC, Canada; 
c Department of Pathology and Laboratory Medicine at the Center for Blood Research, University of British Columbia, Vancouver, BC, Canada; 
d Department of Laboratory Medicine and Pathology, University of Alberta, Edmonton, AB, Canada

Introduction

Plastic bag systems for whole blood collection, component separation, and storage are required for current blood banking practice and transfusion therapies. Bags consisting of different plastic materials are commercially available but polyvinyl chloride (PVC) plasticized with di(2-ethylhexyl) phthalate (DEHP) is the most popular material in use [1]. However, the toxicity of DEHP and congener phthalates has been and remains a topic of public concern [2, 3]. The exposure of transfusion patients to the DEHP that leaches out of PVC blood bags during component storage has been widely discussed [4, 5], with particular concern for pediatric recipients [6, 7]. For red blood cell (RBC) components, replacing DEHP by a non-phthalate PVC plasticizer is challenged by the membrane protective effect that DEHP exerts on RBCs ex vivo. DEHP has been shown to improve stored RBC morphology [8], deformability [9], osmotic fragility [9, 10] and microvesicle release without affecting 2,3-DPG and ATP levels [8]. The enhanced RBC in vivo recovery observed with DEHP [11] underlines the plasticizer’s role in the plasma membrane preservation during storage.

The existing literature identifies n-butyryl-tri-n-hexyl citrate (BTHC), trioctyl-trimellitate (TOTM), and 1,2-cyclohexane-dicarboxylic acid diisononyl ester (DINCH) as the most studied alternatives for a PVC DEHP-free blood collection/storage system [7]. None of these plasticizers are devoid of potential health hazards but DINCH shows the lowest reproductive and developmental toxicity [6], which is also a DEHP-associated risk of concern for pediatric recipients. It has been previously shown that RBCs can be stored satisfactorily in BTHC-plasticized bags [12], despite inferior protection against hemolysis and vesiculation (assessed as the cell-free, membrane-bound protein concentration during storage) compared to DEHP [13]. DINCH has recently
been reported to approach DEHP in terms of protection against hemolysis [14] with the advantage that it leaks less readily from the PVC matrix [15, 16]. Interestingly, little is known about the RBC vesiculation under the influence of DINCH. This study was conducted to examine RBC vesiculation using a paired study including BTHC and DEHP.

Material and Methods

Red Cell Concentrates: Preparation and Shipping
Whole blood (WB) was donated by consenting volunteer research donors at the Canadian Blood Services NetCAD Laboratory, Vancouver, BC, as approved by the Canadian Blood Services Research Ethics Board (Protocol Reference # 2012.008). WB was collected into WB Sang Total Citrate-Phosphate-Dextrose (CPD) 500 ml (± 10%) blood bag sets (Macopharma, Tourcoing, France). WB units were cooled and stored at 20–24 °C on butane-1,4-diol cooling trays. 30 leukoreduced saline-adrenaline-glucose-mannitol (SAGM) red cell concentrate (RCC) units were produced from the WB units according to the buffy coat (top/bottom) method using PVC bags plasticized with DEHP. RCC pairs were pooled (n = 15 pools) and split into three types of pediatric bags: PVC/DEHP (Fresenius Kabi Deutschland GmbH, Bad Homburg, Germany; P459, lot 43FB17CA00), PVC/DINCH (Fresenius Kabi; T2440, lot 43FA10QA00), and PVC/BTHC (Fresenius Kabi; T2440, lot 43FA11QA00), in duplicate. Each bag was filled with 70–75 ml of RCC. One set of RCCs was shipped for testing to Edmonton, AB, in validated shipping containers packed with cold packs and monitored to ensure that the temperature was maintained between 1–10 °C. The other set remained in Vancouver, BC, for testing. All RCCs were stored at 2–6 °C and sampled on days 5, 21, 35, and 42 of storage. At the end of storage, units were assessed for sterility using the BacT/ALERT automated culture system (bioMérieux Canada Inc., St. Laurent, QC, Canada) to ensure that no contamination was introduced as a result of handling.

Supernatant Hemoglobin Concentration
RCCs were sampled (1,000 μl) and centrifuged (2,200 × g, 10 min, 4 °C). 40 μl of the supernatant was transferred to 1,000 μl Drabkin’s reagent, mixed, kept in the dark for 20 min, and then read for light absorption at 540 nm (Spec-tramax Plus 384, Molecular Devices, Sunnyvale, CA, USA). As described elsewhere [17], the absorption intensity was converted to hemoglobin (Hb) concentration based on a reference concentration curve obtained using commercial Hb standards (Stanbio Laboratory, Boerne, TX, USA).

RBC Mean Corpuscular Volume and Mean Corpuscular Hb Concentration
RCC mean corpuscular volume (MCV) and mean corpuscular Hb concentration (MCHC) were determined using an automated cell counter (Coulter AcT, Beckman Coulter, New York, NY, USA).

RBC Deformability
RBC deformability was assessed using a laser-assisted rotational cell analyzer (Mechatronics, Zwaage, The Netherlands) and expressed as the maximum elongation index predicted at infinite shear stress (E_{lim}). Briefly, RBCs were diluted 1:100 in a polyvinyl pyrrolidone solution and subjected to increasing shear stress (0.95, 1.69, 3.00, 5.34, 9.49, 16.87, 30.00 Pa) at 57.0 °C. The deformation pattern produced by the scatter of the laser beam at each stress was plotted as a deformability curve. E_{lim} was obtained using the Eadie-Hofstee transformation, as previously described [18].

Flow Cytometry: Monitoring CD235a, CD47 and Phosphatidylserine (PS) Exposure
Flow cytometry and the use of Trucount tubes (BD Biosciences, San Jose, CA, USA) for glycophrin A-positive (CD235a+) extracellular vesicle (EV) quantification was performed as elsewhere described [19, 20]. Briefly, RBCs were sampled from the units, and 5 μl were diluted with HEPES Ca²⁺ (2.5 mmol/l) buffered saline, pH 7.4, mixed with 5 μl each anti-CD-33235a fluorescein isothiocyanate (FITC), anti-CD47 phosphatidylidethanolamine (PE) and Annexin V-APC, and transferred to Trucount tubes (BD Biosciences). Tubes were incubated for 15 min in the dark at room temperature and then vortexed before analysis using a FACScalibur flow cytometer (BD Biosciences). Forward scatter and side scatter channels were set to log scale to accommodate the visualization of cells and vesicles in a single panel as shown elsewhere [20]. Acquisition was set up on the basis of time (3 min) without gating. For data analysis, the supernatant of a centrifuged RCC sample was used to set an adequate EV gate. RBC EVs were counted as CD235a+ EV-gated events.

Sizing of RCC-Associated EVs Using Dynamic Light Scattering
A Zetasizer Nano S (Malvern, Worcestershire, UK) was used for EV sizing. Uniform polystyrene microspheres of 100, 200 and 400 nm diameter (Bang Laboratories, Fishers, IN, USA) as 0.01% in phosphate-buffered saline (PBS) were used to verify instrument operation. RCCs were sampled (1.5 ml) and centrifuged (2,200 × g, 10 min, 4 °C). Supernatants were collected and re-centrifuged (2,200 × g, 10 min, 4 °C). These supernatants were diluted with two parts of PBS and analyzed using sample refractive index = 1.43 (phospholipid liposomes), dispersant refractive index = 1.33 (water), system temperature = 25 °C, and sample equilibration time = 2 min. The size results were expressed in terms of Z-average.

Osmotic Fragility Assessment
Osmotic fragility was determined for RCCs stored in DEHP-plasticized bags on day 5 and for RCCs in all three bag types on day 43 of storage. Osmotic fragility was assessed at salt (NaCl) concentrations ranging from 0-0.9% as previously described [21]. Hb release was measured by spectrophotometry at 450 nm, with adjustment for albumin and bilirubin interference by absorbance at 380 nm and 415 nm [22].

Pelleting RCC-Associated EVs for Lipid Analysis
RCCs (180 ml) were centrifuged (2,200 × g, 20 min, 4 °C). Supernatants were collected and centrifuged (2,200 × g, 20 min, 4 °C) to remove cell debris. The cell debris-free supernatants were transferred to ultracentrifuge tubes and centrifuged (50,000 × g, 60 min, 4 °C) to precipitate the EVs. The bright red EV pellets obtained were suspended in PBS (500 μl) and stored at −20 °C for up to 16 weeks until required for lipid analysis.

Sample Preparation for Lipid Analysis
PBS-washed RCCs (100 μl) and PBS-stored EVs (100 μl) were spiked with 2 μg each internal standard dimyristoyl glycerophosphoethanolamine (PE 28:0) and dimyristoyl glycerophosphoserine (PS 28:0) and extracted with chloroform/isopropanol, as previously described [23]. The extraction solvents were evaporated using a stream of nitrogen and the extracts were reconstituted in 300 μl MeOH-CHCl₃–20 mmol/l aqueous ammonium acetate (4:1:1, v/v/v) for liquid chromatography-tandem mass spectrometry (LC-MS/MS) analysis.

Reverse Phase LC-MS/MS
LC was performed using a Shimadzu (Kyoto, Japan) system consisting of controller (CBM20Alte), autosampler (SIL20A), two binary solvent pumps (LC20AD), and a column oven (CTO20AC) at 60 °C. Lipid extracts were injected (10 μl) on an Acquity BEH Shield RP18 column (100 × 2.1 mm I.D., 1.7 μm, Waters, Wexford, Ireland) and gradient-eluted with H₂O, 0.1% acetic acid, v/v (mobile phase A) and MeOH (mobile phase B) at a flow rate of 0.3 ml/min. The column outlet was coupled via a Turbo Spray ion source to an API 4000 LC-MS/MS analyzer (AB Sciex, Concord, ON, Canada). LC-MS/MS in the negative mode was applied to obtain precursor ions undergoing a neutral loss (NL) of 87 Da, and LC-MS/MS in the positive mode was applied to obtain precursor ions undergoing a NL of 141 Da. These were used for the selective monitoring of glycerophosphoserine (NL 87) and glycerophosphoethanolamine (NL 141) species. Instrument parameters applied to both ionization modes were: temperature = 450 °C, nebulizer gas (N) = 45 psi, heater gas (N) = 45 psi, curtain gas (N) = 10 psi, declustering potential = 110 V and 20
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Fig. 1. Changes in the concentration of RBC EVs (CD235a+) and supernatant Hb as a function of storage time (A day 5, B day 21, C day 35, D day 42) and blood bag plasticizer (Δ = DEHP, □ = DINCH, ○ = BTHC; n = 15/group; graphs display means ± SD).

Fig. 2. Changes to RBC MCV and supernatant Hb during storage (A day 5, B day 21, C day 35, D day 42) and as a function of the bag plasticizer (Δ = DEHP, □ = DINCH, ○ = BTHC; n = 15/group; graphs display means ± SD).
RCCs stored in BTHC-plasticized bags developed supernatant Hb levels two times higher than those stored in the bags plasticized with DINCH or DEHP (p < 0.001), which consistently had similar levels during storage. Increases in the concentration of Hb in the supernatant were accompanied by increases in the supernatant concentration of RBC EVs (CD235a+). On day 5, the concentration of RBC EVs ranged from $5.0 \times 10^9$ to $9.0 \times 10^9$ EV/l, with the DEHP and BTHC units at the minimum and maximum of this range, respectively (fig. 1A). On day 21, the concentration of RBC EVs had nearly doubled in the DINCH and DEHP groups, whereas the increase in the BTHC group was nearly threefold (fig. 1B), indicating that during the first 3 weeks of storage the rate of vesicle release was higher in the BTHC units (p < 0.001). Starting on day 21, the concentration of RBC EVs was higher in the BTHC units (p < 0.001). For the rest of the storage period, the vesiculation rate was less affected by differences in plasticizer. Between day 21 and day 35, the concentration of RBC EVs increased threefold in all units (fig. 1C); and between day 35 and day 42, a general twofold increase was observed (fig. 1D).

**RBC MCV and Supernatant Hb Correlated Positively**

Supernatant Hb increased with the progression of the storage (fig. 1). Although supernatant Hb increased in all bag types, RBCs stored in BTHC-plasticized bags developed supernatant Hb levels two times higher than those stored in the bags plasticized with DINCH or DEHP (p < 0.001), which consistently had similar levels during storage. Increases in the concentration of Hb in the supernatant were accompanied by increases in the supernatant concentration of RBC EVs (CD235a+). On day 5, the concentration of RBC EVs ranged from $5.0 \times 10^9$ to $9.0 \times 10^9$ EV/l, with the DEHP and BTHC units at the minimum and maximum of this range, respectively (fig. 1A). On day 21, the concentration of RBC EVs had nearly doubled in the DINCH and DEHP groups, whereas the increase in the BTHC group was nearly threefold (fig. 1B), indicating that during the first 3 weeks of storage the rate of vesicle release was higher in the BTHC units (p < 0.001). Starting on day 21, the concentration of RBC EVs was higher in the BTHC units (p < 0.001). For the rest of the storage period, the vesiculation rate was less affected by differences in plasticizer. Between day 21 and day 35, the concentration of RBC EVs increased threefold in all units (fig. 1C); and between day 35 and day 42, a general twofold increase was observed (fig. 1D).

**Results**

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**Fig. 3.** The average size of EVs (unlabeled) on day 5 and on day 42 of storage, as influenced by the bag plasticizer (Δ = DEHP, □ = DINCH, ○ = BTHC; n = 15/group; graphs display means ± SD).

**Fig. 4.** Osmotic fragility of red cell concentrate as influenced by the bag plasticizer. Osmotic fragility was assessed by measuring hemolysis at salt concentrations ranging from 0 – 0.9%. (▲ = DEHP, day 5; △ = DEHP, day 43; □ = DINCH, day 43; and ○ = BTHC, day 43; n = 15; graphs display means ± SD).
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The Average Size of RCC EVs Changed as a Function of Storage Time

The average size of the RCC EVs increased towards 200 nm from day 5 to day 42 of storage in the 3 bag types (p < 0.001; fig. 3), suggesting that in the RCCs there was a mixture of exosomes (50–100 nm) and plasma membrane microvesicles (ectosomes, 200–250 nm) changing in proportion during storage [20], which is consistent with the accumulation of RBC EVs (ectosomes) during storage (fig. 1).

Osmotic Fragility as a Function of Plasticizer

Osmotic fragility curves displayed the characteristic sigmoidal distribution for all samples tested (fig. 4). The curve appeared to shift to the right with increasing storage time suggesting an increase in osmotic fragility of the stored RBCs. For statistical purposes, the amount of hemolysis at a fixed concentration of salt (0.55% NaCl) was selected to interrogate potential differences in osmotic fragility of RBCs stored in the 3 different plastics. At day 43 and at 0.55% NaCl, RBCs stored in BTHC bags displayed the highest hemolysis (mean ± SD 14.1 ± 2.0; range 10.5–17.0; median 14.3), followed by RBCs stored in DINCH bags (mean ± SD 9.6 ± 2.6; range 6.4–14.7; median 9.4), and finally RBCs stored in DEHP bags (mean ± SD 7.6 ± 1.7; range 5.5–11.2; median 7.0; p < 0.01). Regardless of the container, the 43-day stored RBCs all displayed higher hemolysis at 0.55% NaCl than the RBCs stored in DEHP for only 5 days (mean ± SD 1.6 ± 1.0; range 0.5–3.8; median 1.3; p < 0.01).

RBC Deformability as a Function of the RCC Storage

RBCs stored in blood bags plasticized with DEHP, DINCH or BTHC displayed a similar elongation index (EImax) and MCHC on day 5 (fig. 5). On day 21, the ability of RBCs to elongate increased by about 5% (higher EImax) in all bag groups (p < 0.05) while the respective MCHC was decreased by about 5% (p < 0.001), suggesting that cells were more deformable due to a drop in cytoplasmic viscosity. On day 35, although the MCHC continued to decrease, particularly in the BTHC group (3%, p < 0.001), deformability impairments (lower EImax values, p < 0.05) in the order of 2% (DEHP) to 5% (BTHC) were noted. On day 42, all RBCs were less deformable (6–9%) than on day 35 (p < 0.001) despite continued decreases in MCHC, particularly in the BTHC group (4%, p < 0.001).

Phospholipid Analysis

To explore plasticizer-induced changes to the RBC membrane, the distribution of PE and PSs in RBCs and EVs was examined. RBCs stored in bags plasticized with DINCH, BTHC or DEHP were not different in regards to the composition of PEs, lysophosphatidylethanolamines (LPEs) and PSs (fig. 6A, 7A, 8A). Similarly, the EVs accumulated in the respective bags were no different in regards to the composition of the above mentioned lipids (fig. 6B, 7B, 8B). Irrespective of plasticizer, however, the more unsaturated lipids were enriched in the extract of EVs (p < 0.05). These included PEs containing 3 or more carbon-carbon (C-C) double bonds (Δ ≥ 3; fig. 6), LPEs and PSs containing 4 or more C-C double bonds (Δ ≥ 4; fig. 7, 8) particularly.

Fig. 5. Changes to RBC deformability and MCHC as a function of the storage time (A) day 5, (B) day 21, (C) day 35, (D) day 42 and bag plasticizers (Δ = DEHP, □ = DINCH, ○ = BTHC; n = 15/group; graphs display means ± SD). EImax: maximum elongation index predicted at an infinite shear stress.
Discussion

The aim of this study was to compare the RBC membrane preservation capacity of DEHP with the membrane preservation capacity of the alternative plasticizers DINCH and BTHC (citrate). In this paired study (pool-and-split) conducted with leukoreduced RCCs stored in pediatric bags, we found that the membrane stabilization capacity differed among bags manufactured with different plasticizers. Many parameters indicated that, overall, RBCs stored in BTHC-plasticized bags showed poorer membrane preservation capacity than those in DINCH- or DEHP-plasticized bags. A previous study from 1991, found that overall RBC quality in DEHP- and BTHC-plasticized PVC was generally comparable [24]. Our results, focused on events at the RBC membrane, would suggest differently. Irrespective of plasticizer, the data showed a positive correlation between increasing levels of RBC EVs (CD235a+) and supernatant Hb during storage. For these parameters, the plasticizer influenced the rate with which the concentration of EVs and supernatant Hb increased with time. RBC vesiculation levels and rates were similar in DEHP- and DINCH-plasticized bags. In contrast, BTHC-plasticized bags provided less protection against vesiculation, osmotic stress, and Hb loss. By day 21, the levels of vesiculation and supernatant Hb in the BTHC bags were approximately twice as high as those seen in DINCH and DEHP bags. The RBCs stored in BTHC bags also became larger (higher MCV) than those stored in DINCH- or DEHP-plasticized bags, which suggests that the membrane stabilization with DEHP is associated with, but not necessarily limited to, membrane mechanisms in control of RBC volume. The progressive swelling of the RBCs during storage inversely correlated, as expected, with the changes of...
MCHC. These two parameters combined, MCV and MCHC, indicated that the RBCs became less viscous (decreased Hb concentration) with the progression of the storage. Should only viscosity be considered, the RBC deformability should proportionally increase. As shown, all units displayed this simple association up to the 3rd week of the storage. Then, despite lower viscosity, deformability decreased, clearly indicating a storage time point (between the 3rd and 5th week in our study) when changes to the mechanical properties of the membrane made RBCs more rigid. Fundamental changes to the cytoskeleton (e.g. oxidation) and surface area loss due to vesiculation might have at this point become critical. It is thus not surprising that the RCCs presenting more RBC EVs – those stored in PVC-BTHC bags – were also the RCCs containing the most rigid RBCs.

Research by others have demonstrated that exosomes (~50 nm) and microvesicles (~200 nm) from endothelial cells, leukocytes, and platelets exceed the amount of RBC EVs (i.e., microvesicles) in the plasma of healthy individuals (blood donors) [25] as well as in blood bank-produced RCCs as they enter storage [26]. While we did not look at non-RBC EVs in this study, this prior work led us to postulate that the average size increase of the RCC EVs during storage reflected the accumulation of RBC EVs (microvesicles) over exosomes (non-RBC origin) caused by the RBC vesiculation. The measurements of EV size did not capture any particular influence of the plasticizers, suggesting that the analyzed EVs had similar dimensions. Flow cytometry analysis also did not capture any particular influence of the plasticizers on the exposed amounts of PS and CD47 in the RBC EVs. LC-MS analysis also did not capture any particular influence of the plasticizers on the composition of EVs in terms of PEs and PSs, suggesting the presence of a similar membrane asymmetry pattern before vesicle release. The combination of these results suggested that none of the plasticizers exerted a direct interference on the mechanism of vesiculation.

Conclusion

This analysis of EV concentration, size and lipid composition allowed us to conclude that DINCH and DEHP provide equivalent protection to RBCs against vesiculation. In contrast, RCCs stored in BTHC-plasticized bags generated more EVs and had higher levels of supernatant hemoglobin. The RBCs stored in BTHC-plasticized bags were larger, more rigid, and more sensitive to osmotic challenge than RBCs stored in the other containers. Collectively, this data would suggest that DINCH would be a superior alternative to BTHC for replacing DEHP in red cell storage bags. The lack of differences in the composition of PEs and PSs of RBCs and EVs across the plasticizer groups suggested, however, that the protection against vesiculation does not come from a direct intervention on the mechanism of vesiculation. The membrane-protective effect appears to be related to the control of cell swelling.

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**Author Contributions**


**References**


**Disclosure Statement**

This study was a collaboration with Fresenius Kabi Deutschland GmbH, who provided the pediatric bags that were used in this study and reviewed the manuscript before submission. Dr. Dana V. Devine serves on the Fresenius Kabi Deutschland GmbH Expert Panel. The other authors have no conflicts of interest to declare.